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TITLE:

**IMPROVED LONGITUDINALLY FLEXIBLE EXPANDABLE
STENT**

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IMPROVED LONGITUDINALLY FLEXIBLE EXPANDABLE STENT

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EIT This application is a Continuation-in-Part of application Serial No. ~~08/511,076, filed August 3, 1995, the disclosure of which is hereby incorporated by~~

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Field of the Invention

This invention relates to an endoprosthesis device for implantation within a body vessel, typically a blood vessel. More specifically, it relates to a tubular
10 expandable stent of improved longitudinal flexibility.

Background of the Invention

Stents are placed or implanted within a blood vessel for treating stenoses, strictures or aneurysms therein. They are implanted to reinforce collapsing, partially
15 occluded, weakened, or dilated sections of a blood vessel. They have also been implanted in the urinary tract and in bile ducts.

Typically, a stent will have an unexpanded (closed) diameter for placement and an expanded (opened) diameter after placement in the vessel or the duct. Some stents are self-expanding and some are expanded mechanically with radial
20 outward force from within the stent, as by inflation of a balloon.

An example of the latter type is shown in U.S. Patent No. 4,733,665 to Palmaz, which issued March 29, 1988, and discloses a number of stent configurations for implantation with the aid of a catheter. The catheter includes an arrangement wherein a balloon inside the stent is inflated to expand the stent by plastically deforming
25 it, after positioning it within a blood vessel.

A type of self-expanding stent is described in U.S. Patent No. 4,503,569 to Dotter which issued March 12, 1985, and discloses a shape memory stent which expands to an implanted configuration with a change in temperature. Other types of self-expanding stents not made of shape memory material are also known.

30 This invention is directed to stents of all these types when configured so as to be longitudinally flexible as described in detail hereinbelow. Flexibility is a desirable feature in a stent so as to conform to bends in a vessel. Such stents are known in the prior art. Examples are shown in U.S. Patent No. 4,856,516 to Hillstead; U.S.

Patent No. 5,104,404 to Wolff; U.S. Patent No. 4,994,071 to MacGregor; U.S. Patent No. 5,102,417 to Palmaz; U.S. Patent No. 5,195,984 to Schatz; U.S. Patent No. 5,135,536 to Hillstead; U.S. Patent 5,354,309 to Shepp-Pesch et al.; EPO Patent Application 0 540 290 A2 to Lau; EPO Patent Application No. 0 364 787 B1 to Schatz,
5 and PCT Application WO 94/17754 (also identified as German Patent Application 43 03 181).

Generally speaking, these kinds of stents are articulated and are usually formed of a plurality of aligned, expandable, relatively inflexible, circular segments which are interconnected by flexible elements to form a generally tubular body which is
10 capable of a degree of articulation or bending. Unfortunately, a problem with such stents is that binding, overlapping or interference can occur between adjacent segments on the inside of a bend due to the segments moving toward each other and into contact or on the outside of a bend the segments can move away from each other, leaving large gaps. This can lead to improper vessel support, vessel trauma, flow disturbance,
15 kinking, balloon burst during expansion, and difficult recross for devices to be installed through already implanted devices and to unsupported regions of vessel.

A diamond configuration with diagonal connections between each and every diamond of each segment is also known but such closed configurations lack flexibility.

20 It is an object of this invention to provide a longitudinally flexible stent of open configuration that avoids these problems and exhibits improved flexibility (radially and longitudinally) in the stent body segments thereof rather than in flexible joints between the segments.

It is a further object of the present invention to provide a stent that is
25 flexible yet also allows for side branch access.

Summary of the Invention

It is a goal of the present invention to provide a flexible stent formed of interconnected bands which provides for side branch access and which further avoids
30 the problem of pinching or overlap between adjacent bands. Pinching or overlap is avoided where peaks and troughs of adjacent bands are circumferentially displaced relative to each other. The stents of the present invention accomplish this goal by having different bands characterized by different wavelengths over the length of the

stent and/or disposing the interconnecting members in such a way that after expansion of the stent, the phase relationship between adjacent bands is altered with the peaks and troughs displaced circumferentially relative to each other.

The inventive expandable stents are formed of a plurality of
5 interconnected band-like elements characterized by alternating peaks and troughs. The ends of the interconnecting members which join adjacent bands are circumferentially offset and optionally, longitudinally offset. Peaks and troughs in adjacent bands are circumferentially offset as well so that the stent, in an expanded state, will have minimal overlap of peaks and troughs.

10 To this end, the invention provides a tubular, flexible, expandable stent, comprising a plurality of undulating band-like elements of a selected wavelength or wavelengths. The band-like elements have peaks and troughs and are aligned on a common longitudinal axis to define a generally tubular stent body. The peaks and troughs take a generally longitudinal direction along the stent body. Adjacent band-like
15 elements may be in phase or out of phase with each other. The inventive stents further comprise a plurality of interconnecting elements having first ends and second ends. The first and second ends extend from adjacent band-like elements and are displaced from one another in a longitudinal direction and in a radial direction along the stent. Desirably, upon expansion of the stent, at least some of the peaks and troughs of a given
20 band-like element are displaced relative to each other about the periphery of the stent to accommodate longitudinal flexing of the stent within the band-like elements and without interference between adjacent band-like elements.

In one embodiment, two different types of band-like elements are present in the stent, first band-like elements with a first selected wavelength and second band-
25 like elements with a second selected wavelength exceeding the first selected wavelength. The first and second band-like elements preferably alternate over the length of the stent. Although the terminology of 'first band-like element' and 'second band-like element' is used, it is not intended to convey the relative order of appearance of the elements in the inventive stents.

30 In another embodiment, two different types of band-like elements are present, first and second band-like elements, each of which has peaks and troughs. The first band-like elements have more peaks (or troughs) than the second band-like

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elements. Similarly, the invention is also directed to embodiments having first and second band-like elements with peaks and troughs where the peaks (or troughs) of the first band-like elements are spaced closer together than the peaks (or troughs) of the second band-like elements.

5 In another embodiment in which band-like elements of only one wavelength are present, adjacent bands are about 180° out of phase with one another. Interconnecting elements extend at an oblique angle relative to the longitudinal axis from a peak to a trough on an adjacent band.

10 In another embodiment in which band-like elements of only one wavelength are present, peaks from which interconnecting elements emanate are elongated relative to the peaks which are not connected to troughs and similarly, the troughs from which interconnectors emanate are elongated relative to troughs which are not connected to peaks. Further, each interconnecting element extends from the side of a peak to the side of a trough on an adjacent band.

15 In yet another embodiment in which band-like elements of only one wavelength are present, adjacent bands are about 90° out of phase with one another. Each interconnecting element extends between a peak and a trough and the ends of the interconnecting member are circumferentially offset from one another and, optionally, longitudinally offset.

20 The invention further provides a tubular, flexible, expandable stent having a longitudinal axis, comprising one or more cylindrical shaped first segments having first struts, the first segment being defined by a member formed in an undulating pattern of interconnected paired first struts and in which adjacent pairs of first struts in a given first segment are interconnected at opposite ends and one or more cylindrical
25 shaped second segments defined by a member formed in an undulating pattern of interconnected paired second struts and in which adjacent pairs of second struts in a given second segment are interconnected at opposite ends. The first struts are shorter than the second struts. The first segments are formed of a number of first struts and the second segments are formed of a number of second struts with the number of first struts
30 in a first segment exceeding the number of second struts in a second segment. The first and second segments, present and desirably alternating along the stent body, are aligned on a common longitudinal axis to define a generally tubular stent body. Adjacent first and second segments are connected by a plurality of interconnecting elements, each

interconnecting element extending from an end of paired first struts on a first segment to an end of paired second struts on an adjacent second segment. The ends of interconnecting elements are circumferentially offset relative to each other, and optionally, longitudinally offset. Desirably, upon expansion of the stent, the paired
5 struts of the adjacent segments are displaced relative to each other about the periphery of the stent body to accommodate longitudinal flexing of the stent within the segments and without interference between adjacent segments.

Brief Description of the Figures

- 10 Figure 1a shows a band-like element used in the inventive stents.
Figure 1b shows a schematic of a peak region which contains a double peak and a trough region containing a double trough.
- 15 Figure 2 shows a flat view of a stent configuration according to the invention.
Figure 3 shows the pattern of Figure 2 in a tubular stent.
Figure 4a shows a flat view of a stent configuration according to the invention.
Figure 4b shows a flat view of a stent configuration according to the invention.
- 20 Figure 5a shows a flat view of a stent configuration according to the invention.
Figure 5b shows a flat view of a stent configuration according to the invention.
Figure 6 shows a flat view of a stent configuration according to the invention.
- 25 Figure 7 shows a flat view of a stent configuration according to the invention.
Figure 8 shows a flat view of a stent configuration according to the invention.
Figure 9 shows a flat view of a stent configuration according to the invention.
- 30 Figure 10 shows a flat view of a stent configuration according to the invention.

Figure 11 shows a flat view of a stent configuration according to the invention.

Figure 12 shows a flat view of a stent configuration according to the invention.

5 Figure 13 shows the pattern of Figure 12 in a tubular stent.

Figure 14 shows an expanded stent of the configuration shown in Figure 12.

Figure 15 shows a flat view of an alternate stent configuration according to the invention.

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Detailed Description of the Invention

While this invention may be embodied in many different forms, there are described in detail herein specific preferred embodiments of the invention. This description is an exemplification of the principles of the invention and is not intended to
15 limit the invention to the particular embodiments illustrated.

For the sake of consistency, the terms 'peak' and 'trough' shall be defined with respect to the proximal and distal ends of the stent. Each of the stents has a proximal end 91 and a distal end 93 and a longitudinal axis 95, as seen in Fig. 1a. Peaks 36 are generally concave relative to the proximal end of the stent and generally convex
20 relative to the distal end of the stent. Troughs 40, on the other hand, are generally convex relative to the proximal end of the stent and generally concave relative to the distal end of the stent. Notwithstanding this definition, the term peak is also intended to extend to regions 48 that are generally peak-like which may, nevertheless, contain trough-like regions within the peak-like region as seen in Fig. 1b. Similarly the term
25 trough is also intended to extend to regions 52 that are generally trough-like which may, nevertheless, contain peak-like regions within the trough-like region as seen in Fig. 1b.

Corresponding to each peak 36 is an inner diameter peak 38 where the inner diameter of the band-like element reaches its peak. The set of points on a given band-like element which are distal to inner diameter peak 38 is denoted peak region 48.
30 Similarly, corresponding to each trough 40 is an inner diameter trough 42 where the inner diameter of the band-like element reaches its trough. The set of points on a given band-like element which are proximal to inner diameter trough 42 is denoted trough region 52. For the sake of clarity, unless otherwise indicated, analogous portions of

stents will be similarly labeled, using three digit reference numerals to distinguish among the various embodiments shown.

Also included within this definition of peak regions and trough regions are peak regions which are comprised of multiple peaks as well as trough regions which are comprised of multiple troughs such as those shown schematically in Fig 1b. Peak 36 is seen to consist of two sub-peaks 36a,b and trough 40 is similarly seen to consist of two sub-troughs 40a,b. In the case of peaks containing sub-peak and troughs containing sub-troughs, the peak region 48 includes all of the points along the band-like element between the sub-peaks that make up the peak and similarly, the trough region 52 includes all of the points along the band-like element between the sub-troughs that make up the trough.

The inventive stents may incorporate one or more bands of a chosen wavelength. In some embodiments, the inventive stents include one or more small amplitude, short wavelength bands to provide for flexibility and one or more large amplitude, long wavelength bands to give side branch access or to provide for sections of alternative strengths such as soft and/or stiff sections.

Turning to the Figures, Figure 2 shows a flat view of a stent configuration and Figure 3 shows the stent of Figure 2 in tubular form. That is, the stent is shown for clarity in Figure 2 in the flat and may be made from a flat pattern 110 (Figure 2) which is formed into a tubular shape by rolling the pattern so as to bring edges 112 and 114 together (Figure 2). The edges may then be joined as by welding or the like to provide a cylindrical configuration such as that shown generally at 115 in Figure 3.

A more preferred method of manufacture begins with a thin walled tube which is then laser cut to provide the desired configuration. It may also be chemically etched or EDM'd (electrical discharge machined) to form an appropriate configuration.

The configuration can be seen in these Figures to be made up of one or more spaced first band-like elements 120. First band-like elements have a generally serpentine configuration to provide continuous waves to the first band-like elements. The waves are characterized by a plurality of peaks 124 and troughs 128 taking a generally longitudinal direction along the cylinder such that the waves in first band-like elements 120 open as the stent is expanded from an unexpanded state having a first diameter to an expanded state having a second diameter.

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The stent further comprises a plurality of spaced second band-like elements 132 having a generally serpentine configuration to provide continuous waves to the second band-like elements. The waves are characterized by a plurality of peaks 136 and troughs 140 taking a generally longitudinal direction along the cylinder such that the waves in the second band-like elements open as the stent is expanded from an unexpanded state having a first diameter to an expanded state having a second diameter. First and second band-like elements are characterized by respective wavelengths and amplitudes with the wavelength and amplitude of the second band-like elements exceeding the wavelength and amplitude of the first band-like elements.

10 Adjacent first band-like elements 120 and second band-like elements 132 are interconnected via a plurality of interconnecting elements 144. The ends of interconnecting element are circumferentially offset from each other.

 In an embodiment, as shown in Figs. 2 and 3, first band-like elements 120 and second band-like elements 132 alternate over the length of the stent. 15 Optionally, as shown in Figs. 2 and 3, each end 152 of the stent may terminate in a first band-like element. The invention also, however, contemplates each end terminating in a second band-like element, or further, one end terminating in a first band-like element and the other end terminating in a second band-like element.

 While a minimum of one connecting element is required to join adjacent 20 band-like elements, two or more interconnecting elements are preferred. In one embodiment, as shown in Figs. 2 and 3, adjacent first and second band-like elements 120 and 132 are connected with three interconnecting elements 144. Further, in one embodiment, adjacent interconnecting elements 144 extending from peaks 136 on a first band-like element 120 are spaced five peaks apart on the first band-like element while 25 adjacent interconnecting elements 144 extending from troughs 140 on a second band-like element 132 are spaced three troughs apart on the second band-like element.

 It is a further feature of the present invention that peaks 124 on first band-like elements 120 are circumferentially displaced on the periphery of the stent from troughs 140 on adjacent second band-like elements 132. It is desirable that peaks 30 and troughs be displaced in the expanded state of the stent to minimize the possibility of pinching or overlap between adjacent band-like elements.

 Although the stent of Fig. 2 is comprised of two different wavelength band-like elements, the invention contemplates stents with a plurality of different

wavelength band-like elements. As such, other stents may have three, four or more different wavelength band-like elements.

In another embodiment, the inventive stent is comprised of band-like elements of a single wavelength, interconnected by interconnecting elements. Turning
5 to Figs. 4a and 4b, band-like elements 220a,b are interconnected by interconnecting elements 244a,b. Adjacent band-like elements 220a,b are 180° out of phase with one another. In the compressed state, the band-like elements consist of a plurality of peaks 236a,b and troughs 240a,b. Peak region 248a,b and trough region 252a,b have been shaded in one instance for illustrative purposes.

10 In the embodiment shown in Fig. 4a, each interconnecting element 244a extends between a peak region 248a and a trough region 252a. Rectilinear interconnecting elements 244a consist of a first shank 280a, a second shank 284a and a link 288a disposed in-between the first and second shanks 280a and 284a. First shank 280a extends in a longitudinal direction from peak region 248a and is substantially
15 perpendicular to link 288a. Second shank 284a extends in a longitudinal direction from trough region 252a and is perpendicular to link 288a.

In the embodiment shown in Fig. 4b, the stent differs from the embodiment of Fig. 4a in that interconnecting element 244b extending between a peak region 248b and a trough region 252b is curvilinear rather than rectilinear.

20 In both figures 4a and 4b, the interconnecting elements are seen to emanate from the middle of the peak and trough regions.

In another embodiment, as shown in Fig. 5a, the inventive stent is comprised of band-like elements 320a of a single wavelength, interconnected by interconnecting elements 344a. Adjacent band-like elements 320a are 180° out of phase
25 with one another. The band-like elements consist of a plurality of peaks 336a and troughs 340a. Interconnecting elements 344a extend between a peak region 348a and a trough region 352a. The peak regions 348a and trough regions 352a from which interconnecting elements 344a emanate on a given band-like element 320a are seen to extend longitudinally beyond adjacent peak regions 348a' and trough regions 352a' from
30 which no interconnecting elements extend. The extension is such that at least a portion of peak regions 348a overlap longitudinally along the stent with at least a portion of

trough region 352a on an adjacent band-like element 320a'. Of course, the overlap is limited to the longitudinal direction and not to the circumferential direction.

In another embodiment, as shown in Fig. 5b, interconnecting elements 344b extend between peak region 348b and a second closest trough region 352b on an adjacent band-like element. Interconnecting elements 344b are seen to be perpendicular to the longitudinal axis. As in the stent of Fig. 5a, peak regions 348b from which interconnecting elements 344b extend and trough regions 352b from which interconnecting elements 344b extend may extend beyond adjacent peak regions 348b' and trough regions 352b' from which no interconnecting elements 344b emanates.

In another embodiment, as shown in Fig. 6, adjacent band-like elements 420 are in phase with each other. As in previous Figs, band-like elements 420 are of a single wavelength, interconnected by interconnecting elements 444. The band-like elements consist of a plurality of peaks 436 and troughs 440. Interconnecting elements 444 extend at an oblique angle relative to the longitudinal axis of the stent between a peak region 448 and a trough region 452. As such, ends of interconnecting elements 444 are circumferentially offset relative to each other. The exact angle will, of course, depend on the region from which the interconnecting elements extend, as well as on whether interconnecting elements interconnect nearest peaks and troughs, next nearest peaks and troughs or peaks and troughs that are further separated.

In Figures 5a, 5b and 6, the interconnecting elements are seen to emanate from the sides of the peak and trough regions.

Although for the embodiments of Figs. 1-6, the interconnecting elements extend from peak regions on band-like elements to trough regions on adjacent band-like elements, the invention further contemplates interconnecting elements extending from a position between a peak region and an adjacent trough region on a band-like element to a position intermediate a trough region and a peak region on an adjacent second band-like element as in Fig. 7.

In the embodiment of Fig. 7, interconnecting elements are seen to extend from a region between the peak region and the trough region on a band-like element.

The stent is formed of adjacent band-like elements 520 which are 180° degrees out of phase with one another. Interconnecting elements 544 extend from a region intermediate a peak region 548 and a trough region 552 on a band-like element to a

region intermediate a peak region 548 and a trough region 552 on an adjacent band-like element. Interconnecting elements 544 consist of a first shank 560, a second shank 564, and an intermediate member 568 disposed in-between first and second shanks 560 and 564. First shank 560 and second shank 564 are substantially perpendicular to

5 intermediate member 568 which extends in the longitudinal direction. Although not depicted, the region from which interconnecting elements 544 emanate may be midway between peaks and troughs.

The embodiment of Fig. 7 also differs from the embodiments of Figs. 2-6 in the orientation of the interconnecting elements. Whereas the interconnecting
10 elements in Figs. 2-6 are all similarly oriented, in the embodiment of Fig. 7, the orientation of interconnecting elements alternates between adjacent pairs of adjacent band-like elements. Specifically, second shanks 564' of interconnecting elements 544' are seen to be displaced in a clockwise circumferential direction along the stent relative to first shanks 560', and second shank 564" of interconnecting elements 544" are seen
15 to be displaced in a counterclockwise circumferential direction along the stent relative to while first shank 560".

This feature is also seen in the embodiment of Fig. 8 in which adjacent in-phase band-like elements 620 are interconnected by interconnecting elements 644. Interconnecting elements 644 extend at an oblique angle relative to the longitudinal axis
20 of the stent between a peak region 648 and a trough region 652. As in Fig. 7, the orientation of interconnecting elements alternates between adjacent pairs of adjacent band-like elements. Specifically, the distal ends of interconnecting elements 644' are seen to be oriented in a counterclockwise circumferential direction along the stent relative to the proximal end of the interconnecting elements while the distal ends of
25 interconnecting elements 644" are seen to be displaced in a clockwise circumferential direction along the stent relative to the proximal ends.

Although in the embodiments of Figs 2-8, adjacent bands are connected by five interconnecting elements, additional or fewer interconnecting elements may be used. Further, while interconnecting elements are shown spaced three peaks apart and
30 three troughs apart, other separations are contemplated as well.

61 In the embodiment of Figure 9, each band-like element 720 is seen to comprise peaks 736 of more than one amplitude and troughs 740 of more than one

amplitude . Large amplitude peaks 736a and small amplitude peaks 736b alternate as do large amplitude troughs 740a and small amplitude troughs 740b. As in the previous embodiments, the interconnecting elements are oriented at an oblique angle relative to the longitudinal axis 795 of the stent. More generally, the invention is directed at stents
5 comprising band-like elements whose amplitude varies along the band-like element.

In another embodiment of the invention, as shown in Fig. 10, each band-like element 820 is seen to comprise peaks 836 of more than one amplitude and troughs 840 of more than one amplitude, however, peaks of the same amplitude are grouped together within a band-like element as are troughs of the same amplitude. It is further
10 noted that in the embodiment of Figure 10, the location of a group of peaks of given amplitude in a band-like element varies circumferentially along the length of the stent. Interconnecting elements 844 connect peaks 836 and troughs 840 in adjacent band-like elements 820. Where several peaks of different amplitudes are present in a band-like
15 element, the invention further contemplates the possibility of interconnecting elements extending from the large peaks 836a to large troughs 840a as in Fig. 9 as well as the possibility of interconnecting elements extending from large peaks to small troughs or from small peaks 836b to large troughs 840a as in Fig. 10. Further, the interconnecting
20 elements between any two adjacent band-like elements may be of different lengths from one another as seen in Fig. 10 and commence at different longitudinal positions within a band-like element and terminate at different longitudinal positions within a band-like
element. Interconnecting element 844a is seen to be longer than interconnecting element 844b. As in the previous embodiments, the interconnecting elements are oriented at an oblique angle relative to the longitudinal axis 895 of the stent. In the
25 embodiment of Fig. 10, interconnecting element 844a is seen to be oriented at a smaller oblique angle relative to the longitudinal axis of the stent than interconnecting element 844b. As is apparent from Fig. 10, the invention is also directed to stents comprised of
band-like elements whose wavelength varies along a given band-like element. Region 898 and region 899 of band-like element are characterized by different wavelengths.

It is also noted that in the embodiment of Fig. 10, all of the troughs
30 840a,b in a given band-like element 820 are aligned longitudinally along the stent and differ only in their circumferential position along the stent.

It is further noted in the embodiment of Fig. 10, the stent comprises a first group of interconnecting elements 844a and a second group of interconnecting

elements 844b. The interconnecting elements of the first group are all parallel to one another and disposed at a different oblique angle relative to the longitudinal axis than the members of the second group which are all parallel to one another. As such, the invention contemplates stents having several different groups of obliquely disposed
5 interconnecting elements where the oblique angle differs from group to group.

In another embodiment of the invention, as shown in Fig. 11, each band-like element 920 is seen to comprise peaks 936a,b of different amplitudes and troughs 940 of different amplitudes, however, peaks of the same amplitude are grouped together within a band-like element as are troughs of the same amplitude. It is further noted that
10 in the embodiment of Figure 11 the location of groups of peaks of given amplitude in a band-like element varies circumferentially along the length of the stent. Interconnecting elements 944 connect large amplitude peaks 936a and small amplitude troughs 940b in adjacent band-like elements 920. Similarly, interconnecting elements 944 also connect small amplitude peaks 936b and large amplitude troughs 940a.

The invention also contemplates stents similar to that shown in Fig. 11 in which interconnecting elements extend from large peaks 936a to large troughs 940a, as in Fig. 9. Similarly, interconnecting elements may extend from small peaks 936b to small troughs 940b.
15

Further, the interconnecting elements between any two adjacent band-like elements may be of different lengths from one another and disposed at different oblique angles.
20

As is apparent from Fig. 11, the invention is also directed to stents comprised of band-like elements whose wavelength varies along a given band-like element. Region 998 and region 999 of band-like element 920 are characterized by
25 different wavelengths.

It is also noted that in the embodiment of Fig. 11 the large amplitude portions 999 of band-like element 920 are symmetrically disposed about the center 1001 of the band-like element as are the small amplitude portions 998. The center 1001 of the band-like element is defined as a ring that runs along a path that is midway between
30 the large peaks 936a and large troughs 940a of the band-like element. This feature may also be seen in the embodiment of Fig. 9.

The invention is also directed to a tubular, flexible, expandable stent having a longitudinal axis, comprising one or more cylindrical shaped first segments.

Cylindrical shaped first segments 20 as seen in Fig. 1, have first struts 23 having first 25 and second 27 ends. First segments 20 are defined by a member formed in an undulating pattern of interconnected paired first struts 23, in which adjacent pairs of first struts 29' and 29" in a given first segment 20 are interconnected at opposite ends 31' and 5 31", respectively. Adjacent segments are interconnected.

The stent may be seen more clearly in Figs. 2-8. As shown, the stent of Fig. 3, in addition to comprising first segments 120 which are defined by an undulating pattern of interconnected paired first struts 123 in which adjacent pairs of first struts 129' and 129" in a given first segment 120 are interconnected at opposite ends 131' and 10 131", respectively, the stent further comprises one or more cylindrical shaped second segments 132, each second segment being defined by a member formed in an undulating pattern of interconnected paired second struts 135 and in which adjacent pairs of second struts 137' and 137" in a given second segment 132 are interconnected at opposite ends 139' and 139", respectively. First struts 123 are shorter than second struts 135. First 15 segments 120 are formed of a number of first struts 123 and second segments 132 formed of a number of second struts 135, the number of first struts in a first segment exceeding the number of second struts in a second segment. First and second segments 120 and 132 are aligned on a common longitudinal axis 195 to define a generally tubular stent body, shown generally at 115. First and second segments 120 and 132 alternate 20 along the stent body. Adjacent first and second segments 120 and 132 are connected by a plurality of interconnecting elements 144. Each interconnecting element 144 extends from an end 131" of paired first struts on a first segment 120 to an end 139" of paired second struts on an adjacent second segment 132. The ends of interconnecting elements 144 are circumferentially offset relative to each other.

25 Desirably, upon expansion of stent 115, paired struts 129" and 137" of adjacent segments 120 and 132 are displaced relative to each other about the periphery of the stent body to accommodate longitudinal flexing of the stent within the segments and without interference between adjacent segments.

In the embodiments as shown in Figs. 4a, b, cylindrical shaped segments 30 220a,b are formed of interconnected struts 223a,b having first 225 and second 227 ends. Adjacent pairs of struts 229a,b' and 229a,b" in a given segment 220a,b are interconnected at opposite ends 231a,b' and 231a,b", respectively. Adjacent segments are connected by a plurality of interconnecting elements 244a,b. Each interconnecting

element 244a,b extends from an end of paired struts 231a,b" on a segment to an end of paired struts 231a,b' on an adjacent segment. First end 245a,b and second end 247a,b of interconnecting elements 244a,b are seen to be circumferentially displaced along the stent.

5 Similar structure, denoted by similar reference numerals may be found in the stents of Figs. 5a,b, and 6-8.

 In particular, in the embodiment as shown in Fig. 8, cylindrical shaped segments 620 are formed of interconnected struts 623, having first 625 and second 627 ends. Segments 620 are defined by a member formed in an undulating pattern of
10 interconnected paired struts 623 in which adjacent pairs of struts 629' and 629" in a given segment 620 are interconnected at opposite ends 631' and 631", respectively. Segments 620 are aligned on a common longitudinal axis 695 to define a generally tubular stent body. Adjacent segments are connected by a plurality of interconnecting elements 644 (and 644') having first 645 (645') and second 647 (647') ends, each
15 interconnecting element 644 (644') extending from an end of paired struts 631" on a segment to an end of paired struts 631' on an adjacent segment. First end 645 (645') and second end 647 (647") are seen to be circumferentially displaced along the stent.

 Additional embodiment of the stents are shown in Figs 12-15. Figure 12 and Figure 13 show a fragmentary flat view of an unexpanded stent configuration
20 and the actual tubular stent (unexpanded), respectively. That is, the stent is shown for clarity in Figure 12 in the flat and may be made from a flat pattern 1110 (Figure 12) which is formed into a tubular shape by rolling the pattern so as to bring edges 1112 and 1114 together (Figure 12). The edges may then joined as by welding or the like to provide a configuration such as that shown in Figure 13.

25 The configuration can be seen in these Figures to be made up of a plurality of adjacent segments generally indicated at 1116, each of which is formed in an undulating flexible pattern of substantially parallel struts 1118. Pairs of struts are interconnected at alternating end portions 1119a and 1119b. As is seen in Figure 12, the interconnecting end portions 1119b of one segment are positioned opposite
30 interconnecting end portions 1119a of adjacent segments. The end portions as shown are generally elliptical but may be rounded or square or pointed or the like. Any configuration of end portions is acceptable so long as it provides an undulating pattern, as shown. When the flat form 1110 is formed into an unexpanded tube as

shown in Figure 13, the segments are cylindrical but the end portions 1119 of adjacent segments remain in an opposed position relative to each other.

A more preferred method of manufacture begins with a thin walled tube which is then laser cut to provide the desired configuration. It may also be chemically
5 etched or EDM'd (electrical discharge machined) to form an appropriate configuration.

Interconnecting elements 1120 extend from one end portion 1119 of one segment 1116 to another end portion 1119 of another adjacent segment 1116 but not to an oppositely positioned end portion 1119 of an adjacent segment 1116. There
10 are at least three struts included between the points on each side of a segment 1116 at which an interconnecting element 1120 contacts an end portion 1119. This results in the interconnecting elements 1120 extending in an angular direction between segments around the periphery of the tubular stent. Interconnecting elements 1120 are preferably of the same length but may vary from one segment to the other. Also, the
15 diagonal direction may reverse from one segment to another extending upwardly in one case and downwardly in another, although all connecting elements between any pair of segments are substantially parallel. Figure 12, for example shows them extending downwardly, right to left. Upwardly would extend up left to right in this configuration.

20 As a result of this angular extension of the interconnecting elements 1120 between adjacent segments and loops, upon expansion of the stent as seen in Figure 14, the closest adjacent end portions 1119 between segments 1116 are displaced from each other and are no longer opposite each other so as to minimize the possibility of binding or overlapping between segments, i.e., pinching.

25 The number of interconnecting elements 1120 may vary depending on circumstances in any particular instance. Three per segment are satisfactory for the configuration shown and at least three will be used typically.

The alternate design shown in Figure 15 includes longer struts 1118a in the two end segments 1116a than in the intermediate segments 1116. This allows the
30 end segments (1116a) to have less compression resistance than the intermediate segments (1116), providing a more gradual transition from the native vessel to the

support structure of the stent. Otherwise, the configuration is the same as that shown in Figure 12.

As indicated in the Figures, the invention contemplates a variation of interconnecting element shapes ranging from rectilinear to curvilinear. The invention
5 further contemplates embodiments in which all interconnecting elements are similarly oriented as well as embodiments in which adjacent sets of interconnecting elements extending between adjacent pairs of segments are oppositely oriented (e.g., Figs 7 and 8). The invention also contemplates the use of interconnecting elements which extend from a range of positions along the segments, ranging from various positions in the area
10 in which paired struts are interconnected to other positions along the struts.

The invention also contemplates the possibility of interconnecting elements extending at an oblique angle relative to the longitudinal axis of the stent and connecting adjacent peaks and troughs on adjacent segments as well as peaks and troughs on adjacent segments which are separated by one or more peaks and/or troughs.

15 The invention also contemplates reversing the orientation of interconnecting elements as shown in Figs. 7 and 8.

Finally, there are preferably at least three interconnecting elements joining adjacent first and second segments although fewer or additional interconnecting elements are also contemplated.

20 It is understood that the peaks and troughs of the present invention need not be rounded, as shown in the Figures. The peaks and troughs may be bulbous, triangular, square, pointed, or otherwise formed of interconnected straight sections.

As already indicated, this invention is applicable to self-expanding configurations, mechanically expandable configurations and to a wide variety of
25 materials, including both metal and plastic and any other material capable of functioning as an expandable stent. For example, the stent may be of metal wire or ribbon such as tantalum, stainless steel or the like. It may be thin-walled. It may be of shape memory alloy such as Nitinol or the like, etc. The interconnecting elements may be formed integrally with the band-like elements (or segments) or may be bonded thereto via such
30 methods as adhesive bonding, welding or any other known method of bonding.

The above Examples and disclosure are intended to be illustrative and not exhaustive. These examples and this description will suggest many variations and alternatives to one of ordinary skill in this art. All these alternatives and variations are

intended to be included within the scope of the attached claims. Those familiar with the art may recognize other equivalents to the specific embodiments described herein which equivalents are also intended to be encompassed by the claims attached hereto.